



Harmonic Embeddings for Linear Shape Analysis

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Abstract. We present a novel representation of shape for closed contours in \mathbb{R}^2 or for compact surfaces in \mathbb{R}^3 explicitly designed to possess a linear structure. This greatly simplifies linear operations such as averaging, principal component analysis or differentiation in the space of shapes when compared to more common embedding choices such as the signed distance representation linked to the *nonlinear* Eikonal equation. The specific choice of implicit linear representation explored in this article is the class of harmonic functions over an annulus containing the contour. The idea is to represent the contour as closely as possible by the zero level set of a harmonic function, thereby linking our representation to the *linear* Laplace equation. We note that this is a local representation within the space of closed curves as such harmonic functions can generally be defined only over a neighborhood of the embedded curve. We also make no claim that this is the only choice or even the optimal choice within the class of possible linear implicit representations. Instead, our intent is to show how linear analysis of shape is greatly simplified (and sensible) when such a linear representation is employed in hopes to inspire new ideas and additional research into this type of linear implicit representations for curves. We conclude by showing an application for which our particular choice of harmonic representation is ideally suited.

1. Introduction

The analysis and representation of shape is at the basis of many visual perception tasks, from classification and recognition to visual servoing. This is a vast and complex problem, which we have no intention of

addressing in its full generality here. Instead, we concentrate on a specific issue that relates to the representation of closed, planar contours or compact surfaces in 3D space. Even this issue has received considerable attention in the literature. In particular, in their work on statistical shape influence in segmentation [20],

Leventon et al. have proposed representing a closed planar contour as the zero level set of a function in order to perform linear operations such as averaging or principal component analysis. The contour is represented by the embedding function, and all operations are then performed on the embedded representation. They choose as their embedding function the signed distance from the contour (whose differential structure is described by the *non-linear* Eikonal Equation) and implement its evolution in the numerical framework of level sets pioneered by Osher and Sethian [27].

While this general program has proven effective in various applications, the particular choice of embedding function presents several difficulties, because signed distance functions are not a closed set under linear operations: the sum or difference of two signed distance functions is not a signed distance function (an immediate consequence of their nonlinear differential structures). Consequently, the space cannot be endowed with a probabilistic structure in a straightforward manner, and repeated linear operations, including increments and differentiation, eventually lead to computational difficulties that are not easily addressed within this representation. Alternative methods that possess a linear structure rely on parametric representations. For instance various forms of splines [6, 7], cannot guarantee that topology (or even the embeddedness) of the shape is preserved under significant variations of the control points. Furthermore, such representations are not geometric as they depend upon an arbitrary choice of parameterization for the contour. Geometricized parametric representations utilizing the arclength parameter suffer from the same nonlinearity problem as implicit representations utilizing the signed distance to the curve. While it is possible to generalize the notions of mean shapes and PCA to nonlinear representations, especially when they can be endowed with a Riemannian structure, (see for example [17]), it is decidedly more complicated and often involves rather expensive computational algorithms.

In this paper, we present a novel implicit representation of shape for closed planar contours and compact surfaces in \mathbb{R}^3 that is geometric and explicitly designed to possess a (locally) linear structure. This allows linear operations such as principal component analysis or differentiation to be naturally defined and easily carried out. The basic idea consists of, again, representing the contour or surface as the zero level set of a function,

but this time the function belongs to a linear (or quasi-linear¹) space. While previous methods relied on the (non-linear) Eikonal equation, ours relies on Laplace equation, which is linear. Our representation allows exploring the neighborhood of a given shape while guaranteeing that the topology and the embeddedness of the original shape is preserved, even under large variations of the parameters in our representation (the boundary values of the harmonic function).

We should point out that the primary goal here is to show through an example how a linear implicit representation of contours or surfaces can simplify (and justify) linear operations such as averaging and principle component analysis. It is not our claim that the use of Laplace's equation is the optimal choice. It is, however, a well studied PDE whose known properties allow us to conclude various analytical and topological properties of the curves we seek to represent. Further some recent attention to shape analysis via Riemannian structures based on nonlinear representations of curves using harmonic functions is presented in [29] (The authors wonder, in fact, if the linear representation presented here may be tied to of local linearization of this representation in the neighborhood of a given shape). We also show in Section 5 an application that is ideally suited for our particular choice of harmonic embedding. Beyond these considerations, however, most of what we are illustrating in this work could carry through for other classes of linear or quasilinear embedding functions.

We introduce the simplest form of harmonic embedding in Section 2, where we point out some of its difficulties. We then extend the representation to a related anisotropic operator in Section 3, and discuss its finite-dimensional implementation in Section 4. In Section 5 we show an application to measuring tissue thickness on segmented medical image data. Finally, we illustrate some of the properties of this representation in Section 6. While the detailed discussion is restricted to the 2D case, the extension to 3D is straight-forward and obvious. We therefore will make not repeat the same details in 3D, but we will however show 3D examples in the results section.

1.1. Relation to Previous Work

The literature on shape modeling and representation is too vast to review in the limited scope of this paper. It spans at least a hundred years of research in different communities from mathematical morphology

to statistics, geology, neuroanatomy, paleontology, astronomy etc. Some of the earlier attempts to formalize a notion of shape include D’Arcy Thompson’s treatise “Growth and Form” [32], the work of Matheron on “Stochastic Sets” [24] as well as that of Thom, Giblin and others [8, 31]. The most common representations of shape rely on a finite collection of points, possibly defined up to equivalence classes of group actions [5, 13, 19, 23]. These tools have proven useful in contexts where distinct “landmarks” are available, for instance in comparing biological shapes with distinct “parts.” However, comparing objects that have a different number of parts, or objects that do not have any distinct landmark, is elusive under the aegis of statistical shape spaces. Koenderink [18] is credited with providing some of the key ideas involved in formalizing a notion of shape that matches our intuition. However, Mumford has critiqued current theories of shape on the grounds that they fail to capture the essential features of perception [26].

“Deformable Templates,” pioneered by Grenander [11], do not rely on “features” or “landmarks;” rather, images are directly deformed by a (possibly infinite-dimensional) group action and compared for the best match in an “image-based” approach [38]. Another line of work uses variational methods and the solution of partial differential equations (PDEs) to model shape and to compute distances and similarity. In this framework, not only can the notion of alignment or distance be made precise [3, 15, 25, 28, 37], but quite sophisticated theories that encompass perceptually relevant aspects can be formalized in terms of the properties of the evolution of PDEs (e.g. [16]). The work of Kimia et al. [14] describes a scale-space that corresponds to various stages of evolution of a diffusing PDE, and a “reacting” PDE that splits “salient parts” of planar contours by generating singularities. [14] also contains a nice taxonomy of existing work on shape and deformation and a review of the state of the art as of 1994.

The variational framework has also proven very effective in the analysis of medical images [21, 22, 33, 36]. Although most of the ideas are developed in a deterministic setting, many can be transposed to a probabilistic context. Scale-space is a very active research area, and some of the key contributions as they relate to the material of this paper can be found in [1, 2, 12, 30] and references therein. Leventon et al. [20] perform principal component analysis in the aligned frames to regularize the segmentation of regions with low contrast in brain images. Similarly, [35]

performs the joint segmentation of a number of images by assuming that their registration (stereo calibration) is given.

We present a novel representation of shape that supports linear operations. We only consider closed planar contours, and even within this set our representation cannot capture any shape; it does not include a notion of hierarchy or compositionality, which are crucial in a complete theory of shape. Despite its limitations that restrict the class of shapes and the analysis to their global properties, our representation has desirable features when it comes to linear analysis. In fact, it allows us to naturally take linear combinations of shapes; performing principal component analysis (PCA) on the embedding function results in a natural notion of deformation on the underlying shapes. Endowing the space with a probabilistic structure, although not addressed in this paper, is greatly facilitated by the (quasi-)linear nature of the representation.

We note that, although we represent a contour as the zero level set of an embedding function, our approach is not a level set method in the traditional sense [27]: in fact, in local shape analysis we are interested in guaranteeing that changes of topology do *not* occur. In this sense, our approach is far less general, but in ways that are desirable for the specific problem we address, that of representing a neighborhood of a given shape.

As we will see in Section 4, our approach relies on a finite-dimensional set of boundary values at specified locations. In this sense, therefore, our technique could be thought of as an implicit version of splines [6, 7], in the sense that changing the location of the control points results in an evolution of the contour.

2. Harmonic Embedding

The basic idea is to represent a closed planar contour, γ , as the zero level set of a function u that inherits the linear structure of its embedding space. This linear space is chosen to be the set of harmonic functions, which naturally leads to the contour being represented as the solution of certain Laplace equations. More formally, consider the domain $\Omega \doteq \{x \in \mathbb{R}^2 : r < |x| < R\}$; we will restrict our attention to contours that are contained in such a domain, for some $r, R \in \mathbb{R}$. In particular, we will consider smooth contours $\gamma \in \mathcal{C}_\Omega \doteq C^\infty(S^1, \Omega)$ from the unit circle to Ω . We call the inner and outer boundaries of Ω , $\partial_0\Omega \doteq \{x \in \mathbb{R}^2 : |x| = r\}$ and $\partial_1\Omega \doteq \{x \in \mathbb{R}^2 : |x| = R\}$ respectively. Each contour is

then represented by a function $u : \Omega \rightarrow \mathbb{R}$, and in particular by the value of this function in the inner and outer boundaries $\mathfrak{h}_\Omega \doteq C^0(S^1) \times C^0(S^1)$. Among all possible u , we restrict our attention to *harmonic functions*, i.e. to the set $\mathbb{H}_\Omega \doteq \{u \in C^\infty(\Omega) \cap C^0(\bar{\Omega}) : \Delta u = 0\}$.

Definition 2.1. (Harmonic Embedding). We say that a contour $\gamma \in \mathcal{C}_\Omega$ has an *harmonic embedding* if there exists a function $u \in \mathbb{H}_\Omega$ such that

$$\begin{cases} u(x) = 0 \text{ for } x \in \gamma, \\ u(x) \neq 0 \text{ for } x \in \bar{\Omega} \setminus \gamma. \end{cases} \quad (1)$$

We say that the function u is an harmonic representation associated to γ . The set of contours that admit an harmonic embedding will be indicated by \mathcal{C}_Ω^* . We say that $u \in \mathbb{H}_\Omega$ represents an harmonic contour if the zero level set of u is an element of \mathcal{C}_Ω^* . The set of all the harmonic representations will be indicated by \mathbb{H}_Ω^* .

In plain words, we plan to represent a contour γ by the values that a harmonic function u , that is zero on the contour, takes on the inner and outer boundaries $\partial_0\Omega, \partial_1\Omega$. Naturally, not all contours admit a harmonic embedding.

Proposition 2.1. *If $\gamma \in \mathcal{C}_\Omega^*$ and $u \in \mathbb{H}_\Omega^*$ is an harmonic function associated to γ , then u has a constant sign on each connected component of the boundary, $\partial_0\Omega$ and $\partial_1\Omega$, where it takes opposite signs.*

Proof: The function u cannot be zero on the boundary of Ω , because γ does not belong to $\partial_0\Omega \cup \partial_1\Omega$ and the function u is continuous. This implies that it has constant sign on each connected component of the boundary. If u has the same sign on both the connected components of the boundary, then the zero level set must be empty as a consequence of the maximum principle. \square

The relevance of this proposition is that, if we assign negative values to u on the inner boundary and positive values on the outer boundary, the maximum principle guarantees that the resulting zero level set is always simply connected. This is desirable in local shape analysis since we do not want small perturbations of a contour to result in changes of topology. Note that this feature is quite different than traditional level set methods that address more general deformations where changes of topology are desirable. Due to the uniqueness of solution to the Laplace equation, knowing u is

equivalent to knowing its values at the boundaries of the set Ω . Therefore, we can use as a representative of γ not the entire u , but the values f_0 and f_1 that u takes at the boundaries.

Definition 2.2. (Boundary representation). Let $\mathfrak{h}_\Omega^* \subset \mathfrak{h}_\Omega$ such that

$$\mathfrak{h}_\Omega^* \doteq \{(f_0, f_1) \in \mathfrak{h}_\Omega : f_0 < 0, f_1 > 0\}. \quad (2)$$

The elements of \mathfrak{h}_Ω^* are the harmonic shapes and we call the set \mathfrak{h}_Ω^* the harmonic shape space.

The map $\pi_\Omega : \mathbb{H}_\Omega^* \rightarrow \mathfrak{h}_\Omega$ associates to a harmonic function the rescaled boundary values. The map $\psi_\Omega : \mathfrak{h}_\Omega^* \rightarrow \mathcal{C}_\Omega^*$ associates to a rescaled boundary condition the zero level set of the harmonic function with that boundary conditions. The map $h_\Omega : \mathbb{H}_\Omega^* \rightarrow \mathcal{C}_\Omega^*$ associates to a harmonic function in \mathbb{H}_Ω^* its zero level set in \mathcal{C}_Ω^* .

Remark 2.2. The harmonic representation is invariant to scale factors; in fact, if u is the harmonic representation of a contour γ and $\lambda \neq 0$ then also λu is an harmonic representation of γ . Therefore, every contour γ admits an entire equivalence class of embedding functions u , and therefore f_0, f_1 . In order to fix this ambiguity, one can rescale the energy of u , for instance by fixing the value of the integral of $|f_0|, |f_1|$. This will be illustrated in the implementation section (Section 4).

The following proposition guarantees that the representation we have introduced is linear when restricted to \mathfrak{h}_Ω^* . It should also be noted that the set \mathfrak{h}_Ω^* is convex.

Proposition 2.3. (Linearity). *Let $u_1, u_2 \in \mathfrak{h}_\Omega^*$, then there exists a positive number λ such that $u_1 \pm \lambda u_2 \in \mathfrak{h}_\Omega^*$.*

Proof: If we take $\epsilon = \min_{\partial_0\Omega} |u_1|, \mu = \max_{\partial_0\Omega} |u_2|$, then $\lambda = \frac{\epsilon}{2\mu}$ satisfies the requirement. \square

3. Anisotropic Extension

The definitions above indicate that u can be used as a linear embedded representation of γ . However, as we have pointed out, not all contours admit a harmonic embedding. In the experimental Section 6 we give some examples of contours that are not easily captured by the

straightforward harmonic representation. In this section, therefore, we extend the representation to a more general elliptic operator (see [9, 10]) instead of the Laplacian in Eq. (1). In particular we use an operator of the form

$$\nabla \cdot (A(x, y)\nabla u) \tag{3}$$

where $A : \Omega \rightarrow \mathbb{R}^4$ is a differentiable function that associates to each point of the domain a 2×2 matrix. It is immediate to see that if $A(x, y) = I$, the operator (3) reduces to the Laplacian in (1). Naturally, there are infinitely many choices of $A(x, y)$, and this is a power of the representation that is at the disposal of the designer. We choose the following operator:

$$A(x, y) \doteq \frac{1}{\rho^2} \begin{pmatrix} \lambda_1 x^2 + \lambda_2 y^2 & (\lambda_1 - \lambda_2)xy \\ (\lambda_1 - \lambda_2)xy & \lambda_2 x^2 + \lambda_1 y^2 \end{pmatrix} \tag{4}$$

where $\rho = \sqrt{x^2 + y^2}$, λ_1 and λ_2 are two positive constants. The matrix A has the following property:

$$(x, y) \mapsto \lambda_1(x, y), (y, -x) \mapsto \lambda_2(y, -x).$$

This choice may seem to come from “black magic,” but its motivation becomes clear by looking at Fig. 1. In our finite-dimensional implementation, described in Section 4, if we use the harmonic function $\Delta u = 0$, the basis elements are not well localized,² and therefore many coefficients are needed to represent even simple contours. The choice of the operator A above, on the other hand, helps localize and direct the energy of each basis element from the outer to the inner boundary.

4. Finite-Dimensional Implementation

So far we have managed to avoid addressing the problem of how to compute the representation u (or its boundary values f_0, f_1) from the contour γ from either (1) or (3). This is not an easy task, since it is not a standard boundary value problem: one could think of fixing the boundary value at the inner contour to, say, -1 , then solve the Dirichlet problem between $\partial_0\Omega$ and γ , and then attempt to extend u outside γ towards $\partial_1\Omega$. Unfortunately, the analytic continuation of u outside γ is severely ill-posed, and one cannot hope in general to reach the outer boundary for any given contour. A way

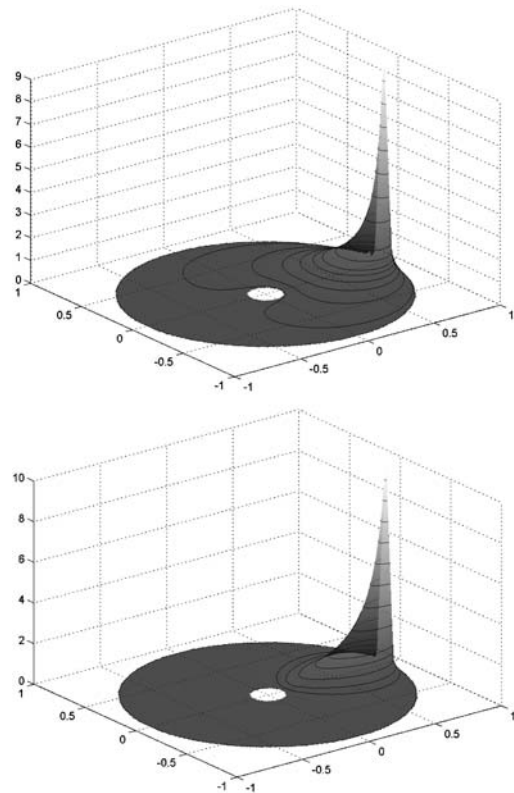


Figure 1. Basis elements according to the model (1) (top), and the more general model with the operator (3) replacing the Laplacian, for $\lambda_1 = 20, \lambda_2 = 1$ (bottom).

to fix this would be to carry out the analytic continuation as far as possible (until a singularity develops) toward the outer boundary, then smooth the resulting analytic boundary values. Next, reverse the procedure to solve the Dirichlet problem between the smoothed outer analytic boundary and the contour γ , and then extend it inward toward the inner boundary. One could iterate the procedure back and forth, which would result in a very laborious and numerically ill-conditioned algorithm to find the representation of a given contour.

In this section, therefore, we seek to approximate γ by the zero level set of a function u that is guaranteed, by construction, to be analytical in Ω . The linear structure of the representation comes handy at this point: in fact, we can seek for functions u of the form

$$u = \sum_{i=1}^n \alpha_{0i} u_{0i} + \alpha_{1i} u_{1i} \tag{5}$$

where u_{0i} and u_{1i} are a set of “basis” functions that are constructed to satisfy Eq. (1) with the operator

(3) replacing the Laplacian, and including the constraints of Remark 2.2 on the inner and outer boundary respectively. More in detail, in order to compute the basis elements, for a chosen positive integer n , we indicate with $\{s_{0j}\}_{1 \leq j \leq n}$ and $\{s_{1j}\}_{1 \leq j \leq n}$ respectively a partition of the inner and outer boundary of Ω , with $|s_{ij}|$ the length of the segment $s_{i,j}$, and seek for $\{u_{ij}\}_{i=0,1;j=1\dots n}$ that solve the following partial differential equation (PDE)

$$\begin{cases} \nabla \cdot (A(x, y)\nabla u_{ij}(x, y)) = 0 & \text{for } (x, y) \in \Omega \\ u_{ij}(x, y) = 0 & \text{for } (x, y) \in \partial\Omega \setminus s_{ij}, \\ u_{ij}(x, y) = \frac{1}{|s_{ij}|} & \text{for } (x, y) \in s_{ij}. \end{cases} \quad (6)$$

We have integrated this PDE numerically using standard finite-element methods [4], and in Fig. 1 we show sample basis elements for the case of the simple Laplacian $A(x, y) = I$ (top), and the more general anisotropic operator (4) (bottom).

Note that this PDE needs only to be solved *once* and off-line. Once the basis elements are known, each contour will be represented by the coefficients $\{\alpha_{ij}\}$, which can be found following the procedure that we describe next.

First, we need to set up a cost functional that measures the discrepancy between the target contour that we want to represent, γ , and the model contour that admits a harmonic embedding. A simple cost function is simply the Lebesgue measure of the set symmetric difference³ between the inside of the contour γ , which we indicate with $\overset{\circ}{\gamma}$, and the set of points that correspond to a negative value of u , which we indicate by u^- . Other choices of cost functional are possible, for instance the Hausdorff distance, and we choose the set symmetric difference only for simplicity. Now, ideally one would want to write this functional explicitly in terms of $\{\alpha_{ij}\}$, and differentiate it to yield a gradient descent algorithm. Unfortunately, it is not easy to write the zero level set of u as a function of the parameters α . However, one can achieve the same results by first computing the gradient flow of the cost functional with respect to an unconstrained u , then projecting this flow onto the basis $\{u_{ij}\}$. More formally, consider a general infinitesimal contour variation $C : [0, 1] \times [-\epsilon, \epsilon] \rightarrow \Omega$; then the gradient descend evolutions of the symmetric difference the target set $\overset{\circ}{\gamma}$ and the approximating set $\overset{\circ}{C}$ is given by

$$C_t = \left(\mathcal{X}_{\overset{\circ}{\gamma}} - \frac{1}{2} \right) N$$

where N is the outward unit normal at $C(\cdot, 0)$ and $\mathcal{X}_{\overset{\circ}{\gamma}}$ is the characteristic function of the set $\overset{\circ}{\gamma}$. After projecting onto the basis elements u_{ij} via $\int_C \langle u_t, u_{ij} \rangle ds$, one obtains the update formula for the coefficients

$$\alpha'_{ij} = \alpha_{ij} - \mu \int_{C(\cdot, 0)} \frac{u_{ij}}{|\nabla u|} \left(\mathcal{X}_{\overset{\circ}{\gamma}} - \frac{1}{2} \right) ds, \quad (7)$$

where μ is a positive constant to be chosen as a design parameter. Finally, one has to enforce the conditions on the sign at the boundary value, described in Proposition 2.1; in this case we simply have:

$$\alpha_{0j} < 0, \quad \alpha_{1j} > 0 \quad \forall j \in \{1, \dots, n\}.$$

We obtain the normalization, with respect to the scale factor of the Remark 2.2, dividing by

$$\sum_{i=1,2;j=1,\dots,n} |\alpha_{i,j}|.$$

Given a target contour γ , this procedure allows us to estimate its representation $\alpha_{i,j}$. In the next section we present some experiments that illustrate the features of this representation.

5. Application to Thickness Estimation for Annular Tissues

In this section we present an application that is ideally suited to harmonic embedding. Namely, harmonic embedding allows a significant improvement in precision for the Eulerian technique for measuring tissue thickness using Laplace's equation [34]. The idea is to generate a harmonic function which is zero on the inner boundary of the tissue and one on the outer boundary of the tissue and then measure the length of the flow lines that move along the gradient from the inner toward the outer boundary. To be more precise, let R be a planar region that is homeomorphic to an annulus (Fig. 2) and $\partial_0 R, \partial_1 R$ be the inner and outer boundary of the region R . Then we define $u : R \rightarrow \mathbb{R}$ as the solution of the following problem:

$$\begin{cases} \Delta u(x, y) = 0 & \text{for } (x, y) \in R, \\ u(x, y) = 0 & \text{for } (x, y) \in \partial_0 R, \\ u(x, y) = 1 & \text{for } (x, y) \in \partial_1 R. \end{cases} \quad (8)$$

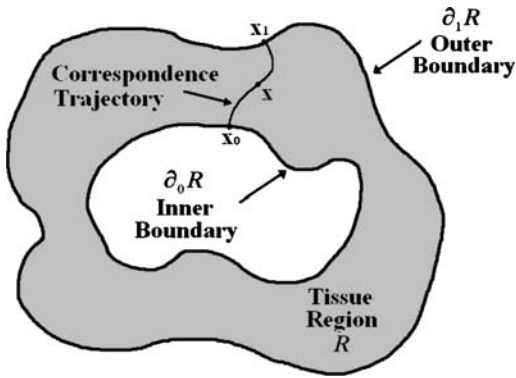


Figure 2. Inner and outer boundaries of the tissue region R and a correspondence trajectory.

To each point $x \in R$, one then associates the unique trajectory which passes through x and which is tangent to the normalized gradient vector field

$$\mathbf{T} = \frac{\nabla u}{|\nabla u|}.$$

The thickness $W(x)$ at the point x is then defined as the length of this correspondence trajectory (Fig. 2). In Fig. 3 there is an example of elliptic region with the corresponding harmonic function u and the tangent field \mathbf{T} . We will now focus on the computation of u .

When implicit representations are employed for the boundaries $\partial_0 R$ and $\partial_1 R$, as occurs when the boundary curves were detected via level set active contours for example, then the boundaries of the annulus R become sub-pixel, making it difficult to enforce the Dirichlet boundary conditions precisely on the inter-pixel boundaries $\partial_0 R$ and $\partial_1 R$. A coarse approximation may be obtained by enforcing the Dirichlet boundary conditions on the first set of neighboring pixel just inside and just outside the annulus, but if higher accuracy is de-

sired in measuring the thickness (particularly in regions where the outer and inner boundary are only a couple pixels apart), then a more accurate solution is required. Harmonic embedding is naturally suited to this task. For the case of $\partial_0 R$, we may assign slightly negative values (rather than 0) to the first set of neighboring pixels inside the annulus and manipulate them to drive the zero level set of u toward the implicitly represented subpixel contour $\partial_0 R$. The nice thing about this is that the contour we are trying to represent ($\partial_0 R$) always lies a fraction of a pixel away from the gridpoints just outside the boundary where the basis functions are computed. As such, it is readily captured by manipulating the basis coefficients as the values of different basis functions are much more distinguishable at points near the boundary compared to points further inside the annulus. A similar procedure is used to enforce the Dirichlet condition on $\partial_1 R$ by assigning values slightly larger than one to the first set of neighboring pixels outside the annulus and manipulating them in order to drive the one level set (rather than the zero level set) of u toward the implicitly represented subpixel contour $\partial_1 R$. Note that we may need to iterate back and forth a few times as changing the values just outside the $\partial_1 R$ boundary may cause slight motions of the zero level set which was obtained by by manipulating the boundary values just outside the $\partial_0 R$ boundary. Given the rapid decay of of the basis functions as one moves further away from their associated boundary coupled with the subpixel vicinity of the two desired contours $\partial_0 R$ and $\partial_1 R$ to their respective boundary pixels, just one or two iterations has always been sufficient in all of our experiments to obtain harmonic functions u with values extremely close to 0 and 1 on the subpixel boundaries $\partial_0 R$ and $\partial_1 R$ using this technique, yielding much more accuracy compared to the simple yet coarse approach of assigning 0 and 1 to the pixels just inside and just outside the annulus respectively.

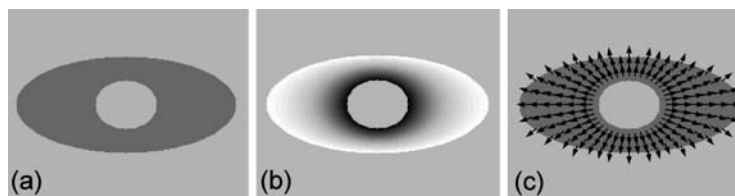


Figure 3. Synthetic annular region between an ellipse and a circle. (a) Elliptic region R . (b) Harmonic function u . (c) Tangent field T .

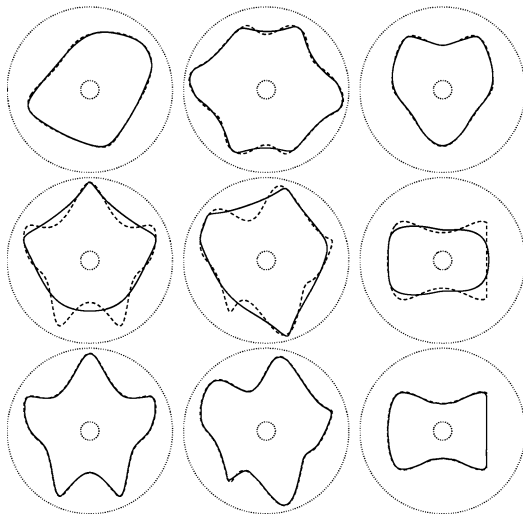


Figure 4. (Top) Original contours (dashed lines) in the domain Ω enclosed between the inner circle $\partial_0\Omega$ and the outer circle $\partial_1\Omega$. The solid line indicates the best approximation based on harmonic embedding (1). The contours in the second row, however, are not as well captured by the simplest representation. Substituting the anisotropic operator (3) instead of the Laplacian results in improved representational power of our scheme (bottom).

6. Experiments

In this section we report some experiments that illustrate the power and limitations of the representation proposed. In Fig. 4 (top) we show a few planar contours (dashed) together with the domain Ω , delimited by the inner and outer boundary circles, and—superimposed—the best approximation of the target contour based on the model (1). While these contours are faithfully captured in the representation, the contours in the second

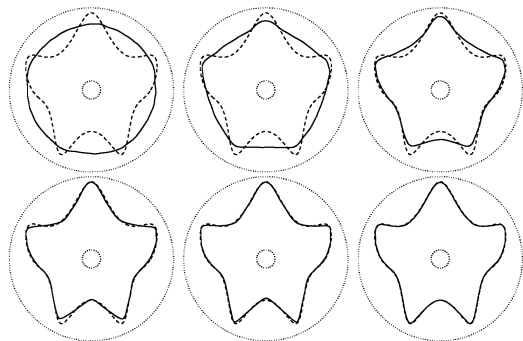


Figure 5. Evolution of an initial estimate (the outer contour) to the minimum of the setsymmetric difference that is used to find the best harmonic embedding.

row are clearly not well approximated. In the following row we show the same target contours and their approximation using the anisotropic operator (3) instead of the Laplacian. As it can be seen, the target contours are much better approximated. Figure 5 shows the evolution of the contour from an initial estimate (the outer boundary) to the minimum of the set-symmetric difference as described in Section 4. One of the strengths of our representation is that it admits a linear structure. Therefore, the computation of increments of a shape (Fig. 6), the average of two or more shapes (Fig. 7) and the analysis of the principal modes of deformation of a shape (Fig. 8) are straightforward to compute. We would like to stress that what is important here is not the result, that is the final *value* of the principal components shown in Fig. 8, but the *procedure* followed to get such principal components. Since our representation is linear by construction, one can simply perform PCA on the coefficients, and automatically get a geometric representation of the deformation that guarantees that no changes of topology occur. Figure 6 is perhaps the most crucial one to illustrate the features of our method. In fact, if we were to use parametric representations of a curve, for instance splines, by perturbing the control points we are not guaranteed that the contour does not develop singularities or self-intersects. Our framework enjoys the benefits of splines in having a finite-dimensional linear representation, but is geometric and perturbations are guaranteed not to result in changes of topology so long as the signs of the basis coefficients (boundary conditions) are maintained.

In Fig. 9 we see an illustration of how the linear structure of this embedding yields natural looking

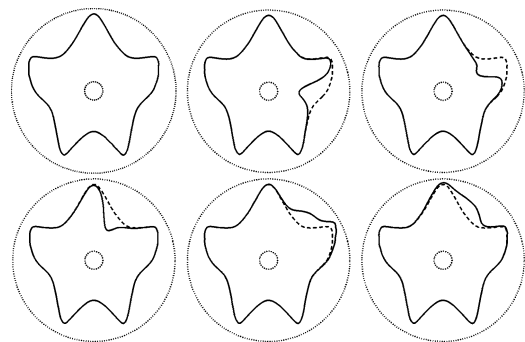


Figure 6. Directional derivatives of a shape can be easily computed in the framework of (anisotropic) harmonic embedding. For the figure in (top-left) we show local perturbations along the direction of five basis elements.

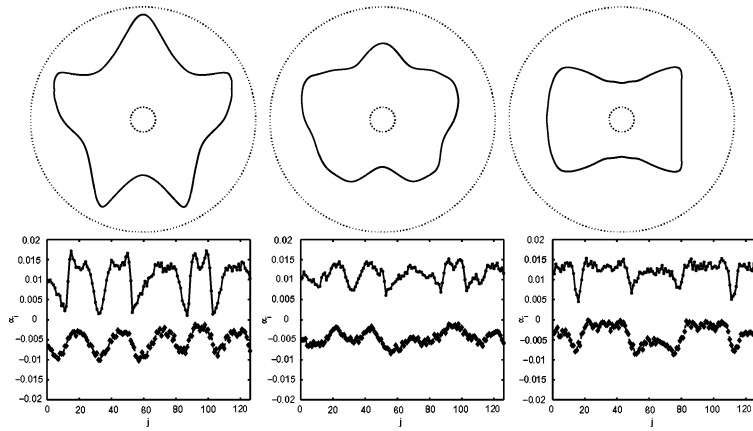


Figure 7. (Top) The average shape between (left) and (right) can be computed by simply averaging (center) the corresponding coefficients (bottom) $\{\alpha_{ij}\}$.

results when employed to compute the mean between two curves, while the non-linear structure of the more popular signed distance embedding yields unnatural looking results when used in the same way. Notice that while both curves are smooth, only the mean harmonic embedding yields a smooth curve whereas the mean signed distance embedding yields a mean curve

with four singular cusps. This should not be surprising since the linearity of the harmonic representation yields an arithmetic mean that is also a harmonic embedding whereas the arithmetic mean of the signed distance representation does not yield another signed distance embedding. As such one may obtain unexpected or undesirable results as seen here when averaging signed distance functions or other nonlinear representations of curves.

We tested the application discussed in Section 5 to evaluate the thickness of annular regions. First we tested with two synthetic regions: circular and elliptic annulus. The results are shown in Figs. 10 and 11. Note that L_0 and L_1 are the partial lengths of the

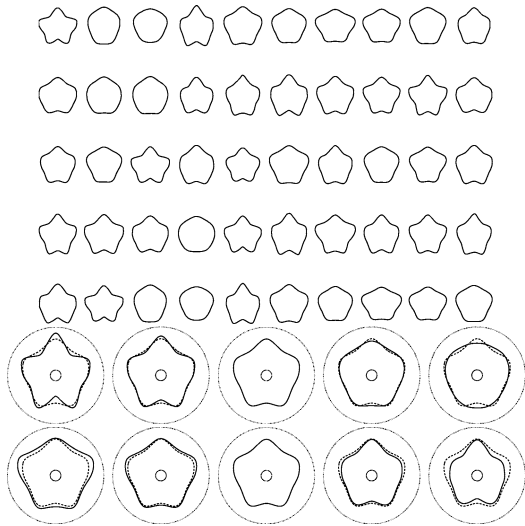


Figure 8. Principal modes of deformation can be easily computed by principal component analysis of the embedded representation. On the top five rows we show a few samples of a collection of shapes. On the bottom in the first row we show the average shape (middle), plus (right) and minus (left) once and twice the first principal component. On the second row we see the effect of the second principal component (left-right) on the mean shape (middle).

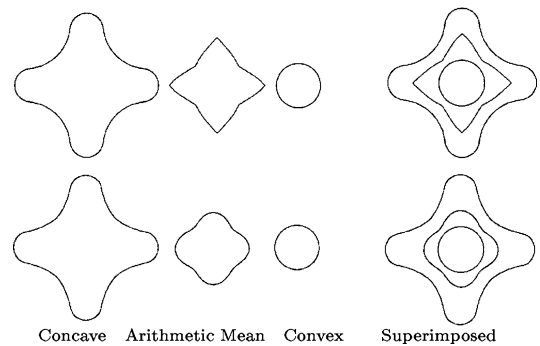


Figure 9. Comparison of “mean curves” (left-center) obtained by taking the zero level set of the arithmetic mean of signed distance (top) and harmonic (bottom) embeddings respectively of a concave (left) and convex (right-center) curve. The two curves and their arithmetic mean are superimposed on the right for both the signed-distance and harmonic case.

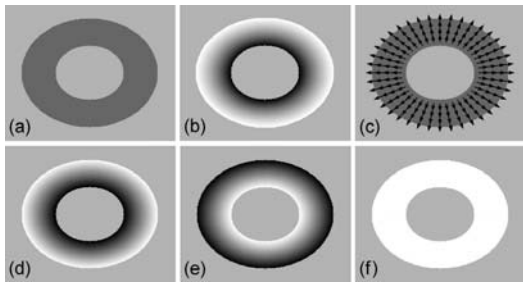


Figure 10. Thickness computations for a synthetic annular region between two concentric circles. (a) Circular annulus. (b) Harmonic function u . (c) Tangent Field. T . (d) Length L_0 . (e) Length L_1 . (f) Thickness ($L_0 + L_1$).

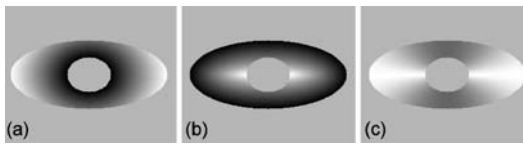


Figure 11. Thickness computations for a synthetic region between an ellipse and a circle. (a) Length L_0 . (b) Length L_1 . (c) Thickness ($L_0 + L_1$).

corresponding flow trajectories between each point x and the boundaries $\partial_0 R$ and $\partial_1 R$ respectively while the thickness is defined by the total trajectory length $L_0 + L_1$. We tested the method also on a segmentation of the myocardium obtained from a short-axis MR image of the heart shown in Fig. 12(a).

Finally, we applied the harmonic embedding representation to a couple of 3-D contours within a spherical annulus. Figures 13 and 14 show the 3-D evolutions of the contours from the initial estimates to the target contours that we want to represent. Figure 15 shows the average shape obtained by just averaging the coefficients. In addition, convex combinations of the harmonic embedding representations can be easily computed by just doing a weighted average of the coefficients to continuously interpolate between the two shapes (Fig. 16).

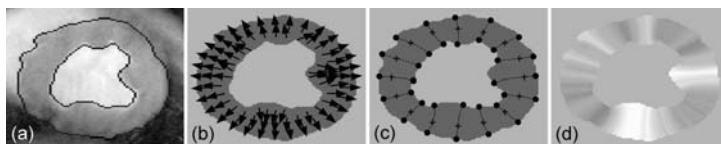


Figure 12. Myocardial thickness from a short-axis MR image. (a) Endocardial and epicardial contours. (b) Tangent field. (c) Boundary correspondences for some selected points. (d) Thickness.

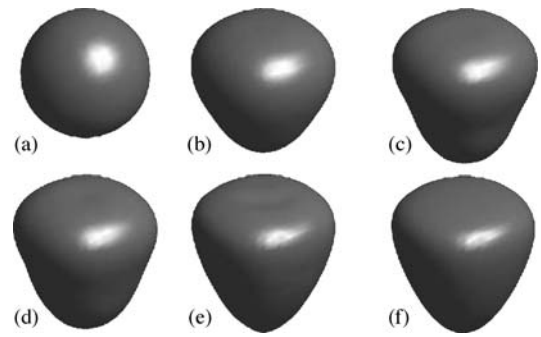


Figure 13. Evolution of an initial estimate to the minimum of the set-symmetric difference that is used to find the best harmonic embedding. (a) Initial contour estimate. (b)–(e) Evolutions. (f) Target contour.

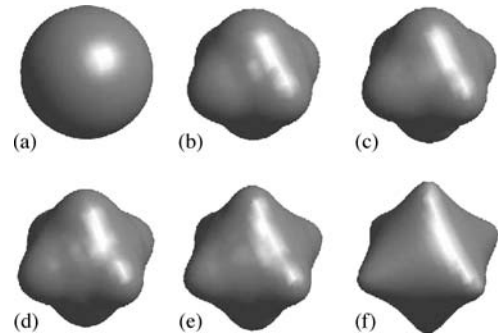


Figure 14. Evolution of an initial estimate to the minimum of the set-symmetric difference that is used to find the best harmonic embedding. (a) Initial contour estimate. (b)–(e) Evolutions. (f) Target contour.

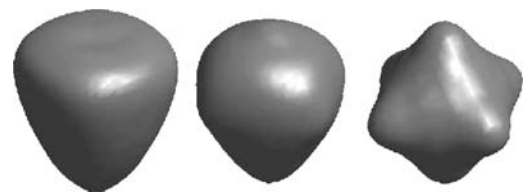


Figure 15. Average shape between (left) and (right) computed by simply averaging (center) the corresponding coefficients.

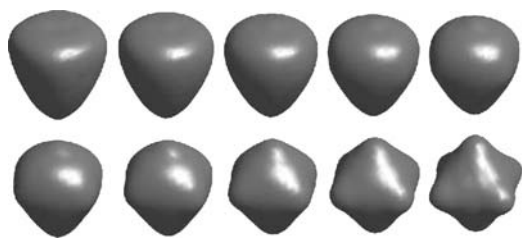


Figure 16. Convex combinations of the two harmonic embedding representations shown in (top left) and in (bottom right).

7. Summary and Conclusions

We have presented a novel representation for the shape of closed planar contours. It does not rely on features or landmark points, and it is characterized by an underlying linear structure that makes linear operations straightforward. We showed examples of computation of the average, increments and principal deformations. Our representation has many shortcomings and it should not be taken as a general tool for shape analysis. It is not invariant with respect to the action of a group (and therefore one has to assume that the shapes are “registered”), it does not possess a notion of compositionality, and it cannot capture many complex contours of practical interest. However, to the best of our knowledge, it is the first and only variational shape representation to possess a linear structure, which is extremely desirable when it comes to numerical implementation of linear operations. An application of a variation of the harmonic embedding to the analysis of the annulus tissues is explained.

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Notes

1. The representation is restricted to a convex subset of a linear vector space.
2. The meaning of the word “basis” will be made precise in the next section.
3. The *symmetric difference* between two set A and B is $A \Delta B = (A \setminus B) \cup (B \setminus A)$.

References

1. L. Alvarez, F. Guichard, P.L. Lions, and J.M. Morel, “Axioms and fundamental equations of image processing,” *Arch. Rational Mechanics*, Vol. 123, 1993.
2. L. Alvarez, J. Weickert, and J. Sanchez, “A scale-space approach to nonlocal optical flow calculations,” in *In ScaleSpace '99*, 1999 pp. 235–246.
3. R. Azencott, F. Coldefy, and L. Younes, “A distance for elastic matching in object recognition,” in *Proc. 13th Intl. Conf. on Patt. Recog.*, Vol. 1, 1996 pp. 687–691.
4. S. Brenner and L. Scott, *The Mathematical Theory of Finite Element Methods*, volume 15, of *Texts in Applied Mathematics*. Springer, 2002.
5. T.K. Carne. “The geometry of shape spaces,” *Proc. of the London Math. Soc. (3) 61*, Vol. 3, No. 61, pp. 407–432, 1990.
6. D. Cremers, F. Tischhäuser, J. Weickert, and C. Schnörr. Diffusion Snakes: Introducing statistical shape knowledge into the Mumford–Shah functional. *Int. J. of Computer Vision*, Vol. 50, No. 3, pp. 295–313, 2002.
7. C. de Boor. *A Practical Guide to Splines*. Springer Verlag, 1978.
8. P. Giblin. *Graphs, Surfaces and Homology*. Chapman and Hall, 1977.
9. E. Giusti. *Metodi diretti nel calcolo delle variazioni*. Unione Matematica Italiana, 1994.
10. E. Giusti. *Partial Differential Equations*, volume 19, of *Graduate Studies in Mathematics*. American Mathematical Society, 1998.
11. U. Grenander. *General Pattern Theory*. Oxford University Press, 1993.
12. P. Jackway and R. Deriche, “Scale-space properties of the multiscale morphological dilation/erosion,” *IEEE Trans. on Pattern Analysis and Machine Intelligence*, Vol. 18, No. 1, pp. 38–51, 1996.
13. D.G. Kendall, “Shape manifolds, procrustean metrics and complex projective spaces,” *Bull. London Math. Soc.*, Vol. 16, 1984.
14. B. Kimia, A. Tannebaum, and S. Zucker, “Shapes, shocks, and deformations I: The components of two-dimensional shape and the reaction-diffusion space,” *Int'l J. Computer Vision*, Vol. 15, pp. 189–224, 1995.
15. R. Kimmel and A. Bruckstein, “Tracking level sets by level sets: A method for solving the shape from shading problem,” *Computer Vision, Graphics and Image Understanding*, Vol. 62, No. 1, pp. 47–58, 1995.
16. R. Kimmel, N. Kiryati, and A.M. Bruckstein, “Multivalued distance maps for motion planning on surfaces with moving obstacles,” *IEEE Trans. Robot. & Autom.*, Vol. 14, No. 3, pp. 427–435, 1998.
17. E. Klassen, A. Srivastava, W. Mio, and S. Joshi, “Analysis of Planar Shapes Using Geodesic Paths on Shape Spaces,” *IEEE Trans. Pattern Anal. & Machine Interp.*, Vol. 26, No. 3, pp. 372–383, 2004.
18. J.J. Koenderink. *Solid Shape*. MIT Press, 1990.
19. H. Le and D.G. Kendall, “The riemannian structure of euclidean shape spaces: A novel environment for statistics,” *The Annals of Statistics*, Vol. 21, No. 3, pp. 1225–1271, 1993.
20. M. Leventon, E. Grimson, and O. Faugeras. Statistical shape influence in geodesic active contours, 2000.
21. R. Malladi, R. Kimmel, D. Adalsteinsson, V.C.G. Sapiro, and J.A. Sethian, “A geometric approach to segmentation and analysis of 3d medical images,” in *Proc. Mathematical Methods in Biomedical Image Analysis Workshop*, 1996 pp. 21–22.
22. R. Malladi, J.A. Sethian, and B.C. Vemuri, “Shape modeling with front propagation: A level set approach,” *IEEE Trans. on Pattern Analysis and Machine Intelligence*, Vol. 17, No. 2, pp. 158–175, 1995.

23. K.V. Mardia and I.L. Dryden, "Shape distributions for landmark data," *Adv. appl. prob.*, Vol. 21, No. 4, pp. 742–755, 1989.
24. G. Matheron. *Random Sets and Integral Geometry*. Wiley, 1975.
25. M.I. Miller and L. Younes, "Group action, diffeomorphism and matching: A general framework. In *Proc. of SCTV*, 1999.
26. D. Mumford, "Mathematical theories of shape: Do they model perception?" In *Geometric methods in computer vision*, Vol. 1570, pp. 2–10, 1991.
27. S. Osher and J. Sethian, "Fronts propagating with curvature-dependent speed: Algorithms based on hamilton-jacobi equations," *J. of Comp. Physics*, Vol. 79, pp. 12–49, 1988.
28. C. Samson, L. Blanc-Feraud, G. Aubert, and J. Zerubia, "A level set model for image classification," in *International Conference on Scale-Space Theories in Computer Vision*, 1999 pp. 306–317.
29. E. Sharon and D. Mumford, "2D-Shape Analysis using Conformal Mapping," in *Conference on Computer Vision and Pattern Recognition*, 2004.
30. B. ter Haar Romeny, L. Florack, J. Koenderink, and M.V. (Eds.), "Scale-space theory in computer vision," in *Lecture Notes in Computer Science*, Vol. 1252. Springer Verlag, 1997.
31. R. Thom. *Structural Stability and Morphogenesis*. Benjamin; Reading, 1975.
32. D.W. Thompson. *On Growth and Form*. Dover, 1917.
33. P. Thompson and A.W. Toga, "A surface-based technique for warping three-dimensional images of the brain," *IEEE Trans. Med. Imaging*, Vol. 15, No. 4, pp. 402–417, 1996.
34. A. Yezzi and J. Prince, "An eulerian pde approach for computing tissue thickness," *IEEE Trans. Medical Imaging*, Vol. 22, pp. 1332–1339, 2003.
35. A. Yezzi and S. Soatto, "Stereoscopic segmentation," in *Proc. of the Intl. Conf. on Computer Vision*, 2001 pp. 59–66.
36. A. Yezzi and S. Soatto, "Deformation: Deforming motion, shape average and the joint segmentation and registration of images," *Intl. J. of Comp. Vis.*, accepted, 2003.
37. L. Younes, "Computable elastic distances between shapes," *SIAM J. of Appl. Math.*, 1998.
38. A. Yuille. "Deformable templates for face recognition." *J. of Cognitive Neurosci.*, Vol. 3, No. 1, pp. 59–70, 1991.